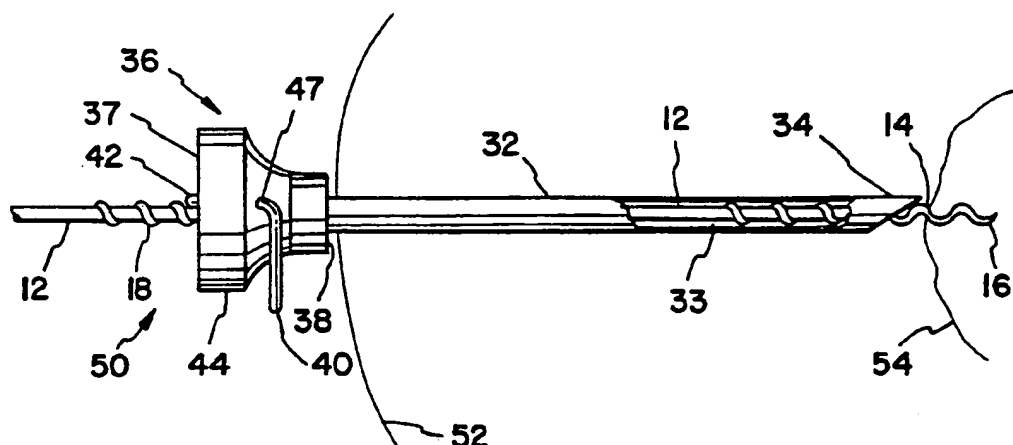




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(54) Title: LESION LOCALIZATION DEVICE AND METHOD OF USING**(57) Abstract**

A lesion localization marking wire (10) and needle assembly (30) for marking non-palpable lesions within the body. A marking device (10) having a helically wound coil of wire (14) attached to an end of the shaft (12) which is insertable into the body through a needle or cannula (30) for rotatably anchoring the marking device (10) into a lesion or tumor (54) is provided. The needle or cannula (30) is inserted into the body with the marking device (10) positioned therein so that when the cannula is positioned proximate to a lesion (54) the shaft (12) of the marker is rotated to advance the marker (10) into the lesion to mark it for subsequent surgical procedures. A second helical wire (18) may be provided on the shaft (12) which cooperates with a wire guide device (40) attached to the needle (30) to enable the physician to determine the depth of the marking device (10) as it anchors into the lesion (54). In particular, the device is provided for marking for biopsy lesion of the breast.

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- 1 -

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LESION LOCALIZATION DEVICE AND METHOD OF USING

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The present invention relates to lesion localization needles and devices, for use in localizing or marking non-palpable lesions and tumors within the body, and more particularly, the present invention relates to a needle assembly which includes a wire marker having a helically wound wire tip for rotatably anchoring a marker to a lesion within a human breast.

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Localization or marking of lesions within the body, such as non-palpable lesions discovered within the body, and devices such as needles and wires for marking these lesions, are well known in the art. The devices generally comprise a hypodermic needle or cannula which is inserted into the body under local anesthesia to a position adjacent and in contact with the lesion. The wire marker is then passed through the cannula and is anchored into the lesion so that the lesion is marked for subsequent surgical procedures such as excision or biopsy. After marking the lesion with the wire marker, the cannula is usually removed from the body, leaving the wire in place and extending from the body. However, these markers tend to dislodge and migrate during transport of the patient for the surgical biopsy procedure.

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Increasingly, ultrasonic imaging is being used as a preferred ancillary or adjunctive imaging method to evaluate breast masses which may be associated with positive or negative mammographic findings. Currently available localization and marking devices image poorly, if at all, ultrasonically, making it difficult to accurately pinpoint

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-2-

the tip of the localization wire with respect to the lesion.
1 Consequently, a subsequent surgical biopsy procedure may
result in an inaccurate incision causing unnecessary tissue
damage, and may necessitate a second surgical procedure to
properly biopsy the lesion, causing the patient unnecessary
5 pain, suffering, and expense.

In the prior art, several types of lesion
localization devices and lesion markers are disclosed.
Currently, the method of detecting and performing a biopsy on
10 a non-palpable occult lesion within the body, such as
non-palpable breast lesions, has been to radiologically or
ultrasonically locate the lesion and to mark the lesion using
a localization needle assembly, prior to a biopsy procedure.
These needle assemblies generally comprise a hypodermic
15 needle or cannula which is inserted into the body to an area
adjacent to and in contact with the lesion. A marking wire
is then inserted through the cannula into the lesion and
anchored in place so that the cannula may be removed.

Ultrasonic imaging is increasingly being used as
20 the preferred method of detection and evaluation of lesions
and masses within the body due to its accuracy, and in view
of the fact that the patient is not exposed to potentially
harmful radiation for extended periods of time. The prior
art marking devices generally image very poorly
25 ultrasonically, as the tip of the previous marker shows up as
a small, hard to locate dot or spot on the viewing screen.
Depth perception is very limited, and consequently, accurate,
reliable placement of the previous marking device is not
guaranteed.

30 Nicholson, et al., U.S. Patent No. 4,616,656,
discloses a probe wire and sheath assembly in which the wire
has a J-type memory hook for marking lesions. The wire probe
has a soft flexibility so that when it is enclosed within the
sheath it has a straight configuration. The sheath, or
35 needle, is inserted into the body, for instance into the

1 breast of a female patient, and positioned proximate to a
2 lesion. The wire probe is then pushed further into the
3 lesion so that the memory hook is reformed and anchors itself
4 within the lesion. The sheath is then removed leaving the
5 hook embedded in the lesion as a marker.

6 A similar device is disclosed in Hawkins, Jr., U.S.
7 Patent No. 4,230,123. Hawkins, Jr. discloses a needle sheath
8 assembly which consists of a small gauge needle in which a
9 stylus or wire is positioned within a cannula. A shorter
10 outer sheath is slidably located over the cannula which is
11 removable after insertion of the needle into the patient's
12 body. The wire has a J-type hook which is passed through the
13 cannula to stabilize the tip of the cannula during biopsy.

14 Nicholson, et al. and Hawkins, Jr. are subject to
15 several disadvantages which effect the accuracy and
16 performance of the device. Devices such as those disclosed
17 in these references image very poorly and are inconsistently
18 visualized ultrasonically, and consequently may not be
19 accurately placed. Furthermore, in procedures involving
20 lesions of the breast, the breast is compressed during the
21 mammographic localization procedure so that after the needle
22 is in place and compression discontinued, the needle marker
23 may inadvertently dislodge or migrate to a different position
24 than that set during the localization procedure. The needle
25 may also deflect away from the lesion, or if the strength and
26 resiliency of the wire is less than that required to
27 penetrate the lesion, the hook may not reform, allowing the
28 marker to migrate or dislodge. This can result in damaging
29 the tissues of the breast, as well as an inaccurate surgical
30 incision during the biopsy procedure, usually requiring a
31 second surgical procedure to properly biopsy the lesion,
32 causing the patient unnecessary pain, suffering and expense.
33 Devices of this type also generally require that the breast
34 be stabilized during transport of the patient from the
35 radiology section of a hospital to the surgical section for
the biopsy procedure in order to prevent dislodgement of the
marker.

Simon, U.S. Patent No. 4,790,329, discloses a
1 biopsy localization device having a sheath or cannula through
which a barbed rod passes. The cannula is provided with
an open side port through which the barb extends upon
positioning within a lesion. In use, the barb is compressed
5 within the lumen of the cannula and the pointed end of the
rod extends from the cannula. As the device penetrates the
patient's body, and into a lesion, the rod is rotated 180° so
that the end of the barb may pass through the open side port
of the cannula. The rod is then drawn back so that barb and
10 cannula anchor into the lesion to prevent removal. While the
device is relocatable, such as by drawing back the cannula to
enclose the barbed rod after anchoring, it is apparent that
some tissue damage will result due to the barb puncturing
the tissue once it is anchored. In addition, the cannula
15 remains in place while the lesion is marked by the barb,
which results in excessive weight applied to the tissue. The
entire device must be stabilized in order to prevent tearing
of tissue and dislodgement of the marker. As related to
breast lesions, as discussed above, compression of the breast
20 during the procedure provides accurate anchoring of the barb;
however, during transport of the patient, the additional
weight of the cannula as well as the barbed rod will require
stabilization of the breast to prevent migration and
dislodgement of the device. A similar device, facing the
25 same disadvantages, is disclosed in Hawkins, et al., U.S.
Patent No. 4,799,495.

An additional type of prior art lesion
localization and biopsy device is commonly referred to as the
"Nordenstrom Screw Diagnostic Instrument", which was
30 developed by Bjorn Nordenstrom (Radiology, November 1975,
Volume 117, Page 474). The Nordenstrom screw is generally a
biopsy device and not a lesion localization and marking

1 device. A cannula is provided which is inserted into the
body, having a screw-tipped rod within the lumen of the
cannula. When the cannula is positioned proximate a lesion,
the rod is rotated to screw the tip into the lesion. The
screw tip is integral with the rod itself, and is a finely
5 machined device in which the screw threads define grooves
which taper to the tip of the device. After the screw tip is
rotated into the lesion, the cannula is then rotated in an
opposite direction using slight forward pressure to a
position over the screw threads. Tissue from the lesion is
10 captured in the grooves of the screw tip and the entire
device is withdrawn so that the tissue may be examined. The
Nordenstrom screw device, as stated above, is not a marking
device, but instead allows the physician to immediately
biopsy the lesion in question.

15 An additional marking device using a screw tip is
disclosed in Hawkins, et al., U.S. Patent No. 4,799,495. In
this device, the cannula may be provided with a tapering
screw tip to anchor the cannula in the tissue while the
needle marker penetrates the lesion. The cannula and wire
20 are used to mark the lesion, and Hawkins et al. also
discloses the use of the cannula alone for marking the
lesion. Furthermore, Hawkins et al. discusses a helical
screw needle marker, similar to the Nordenstrom screw device,
which may be inserted through the cannula to mark the lesion.
25 However, the tapering screw tip of Hawkins et al. is a finely
machined device which is quite expensive to manufacture, and
which also is subject to the disadvantage that the tapered
end may result in the loosening or "backing off" of the screw
tip which will dislodge the marker during transport of the
30 patient, or upon discontinuation of compression of the breast
during the marking procedure. Furthermore, the precise
machining of the tip of this device, and in particular a

1 hollow screw-tipped cannula, would be a difficult and very
expensive procedure from a manufacturing standpoint, and
would necessitate that the device be reusable due to these
cost considerations. In view of this, and in light of
5 current health risks and concerns for patient safety as
related to blood products and invasive surgical procedures,
sterilization procedures would be required prior to and after
each use, thereby making the procedure more elaborate and
expensive than normally necessary.

10 The novel, disposable lesion localization and
marking device of the present invention obviates the problems
associated with the prior art lesion localization devices by
providing an inexpensive, simple to manufacture lesion
marking device having a helically wound marking wire attached
to a wire shaft which passes through a hypodermic needle
15 comprising a cannula. The helically wound marking wire
extends concentrically outward from the shaft and maintains a
substantially uniform diameter so that once the wire is
rotated or screwed into a lesion, it remains anchored in the
tissue without the possibility of backing off and dislodging.

20 In a preferred embodiment, a second helically wound
wire is provided on the shaft remote from the first helically
wound wire at the tip which, in conjunction with a wire guide
provided on a gripping knob of the cannula, assists in the
forward advancement of the shaft so that excessive forward
25 pressure is not required, and the second helix also acts as a
depth guide to provide an accurate indication of the depth to
which the first helix is embedded in a lesion. The helically
wound wires are secured to the shaft by means such as
soldering, or may be wound as part of the shaft itself, so
30 that the entire device is simple to manufacture and
relatively inexpensive, thereby making the device disposable
following the biopsy procedure.

1 The present invention eliminates or substantially
ameliorates the disadvantages encountered in the prior art
through the provision of a lesion localization and marking
device having a helically wound wire tip attached to a shaft
5 which is inserted within the lumen of a cannula into the body
and then rotated into a lesion to anchor the marker within
the lesion tissue. The device is simple to manufacture and
inexpensive thereby making it a disposable unit, which may be
packaged in a sterile packaging unit for one time use.

10 The lesion localization and marking device of the
present invention consists of a marker having a shaft
constructed of stainless steel or other biocompatible
material which has secured to its distal end, or formed
integrally thereon, a stainless steel wire which is helically
15 wound about the end of the shaft. The helically wound wire
extends outwardly in a concentric manner from the end of the
shaft and overhangs the shaft a predetermined distance. The
end of the helix is sharpened to facilitate insertion into a
lesion within the body. The helical wire is secured to the
20 shaft by conventional means such as soldering.

 The marking device, when used in conjunction with
the needle assembly of the present invention, may be provided
with a second helically wound wire which is secured to the
shaft of the marker remote from the end having the first
25 helically wound wire. The second helically wound wire is
secured to the shaft by soldering, or integrally formed as
part of the shaft, and is dimensioned to have the same number
of turns per centimeter as the first helically wound wire,
thus having the same pitch or angle for each turn of coil.
30 The marking device is positioned within a hypodermic needle
or cannula which essentially comprises a stainless steel tube
having a cutting edge at one end and a thermoplastic gripping

1 knob at its other end. The gripping knob has a hole bored
through the center which preferably aligns with the lumen of
the cannula, and a second hole is bored through the knob
parallel to the first hole and offset from the center of the
lumen. Through the second hole is positioned a wire guide
5 which is bent perpendicular to the hole and placed to
partially cover the first hole, leaving an opening which is
substantially equal to the diameter of the shaft of the wire
marker plus the diameter of the wire which forms the helix.

10 In use, the needle assembly is inserted into the
body, such as into the breast of a female patient, until the
tip of the cannula is proximate to a lesion which has been
discovered during a mammographic or ultrasonic imaging
procedure. The marking device is positioned within the
cannula so that the sharpened tip of the first helical wire
15 is adjacent to the cutting edge of the cannula, and the
second helical wire is positioned a predetermined distance
such that the end of the second helical wire closest to the
first helical wire is adjacent to and engages the wire guide
of the thermoplastic knob of the cannula. As the marking
20 device is rotated, the second helical wire is guided along
the wire guide so as to stabilize the shaft while drawing the
marker into the cannula due to the interaction of the second
helix and the wire guide during rotation, and the first
helical wire is rotated into the lesion. The wire guide
25 assists the forward advancement of the marker during
rotation.

The length of the second helical wire is identical
to the length of the first helical wire from the end of the
shaft to the sharpened tip, and both helical wires have an
30 identical number of turns per centimeter. As the first
helical wire is embedded into the lesion, the physician can
accurately gauge the depth to which the first wire enters the
lesion by the distance the second helical wire extends

1 outwardly from the gripping knob of the cannula. When the
second helical wire is fully rotated within the cannula the
physician will know that the first wire is fully extended
outside the cannula and is in position with respect to the
5 lesion. The cannula is then removed from the body leaving
the marking device in place.

As ultrasonic imaging is increasingly being used as
the preferred method of evaluation of breast lesions in
localization procedures, it is very important the the marker
10 used in the localization procedure provide consistent
visualization and clean imaging with a recognizable acoustic
pattern. Prior art markers do not provide adequate
ultrasonic imaging and consequently do not contribute to
accurate localization of a lesion. The present invention,
15 however, due to the helical tip, provides excellent imaging .
characteristics compared to prior art markers, such that each
turn of the helix images distinctly, as opposed to the single
spot or dot appearing from the prior art markers. As a
result, the present marker provides an unambiguous ultrasonic
20 image allowing for accurate marking of the discovered lesion
under the same conditions as mammography, thus reducing the
patient's exposure to X-rays as well as decreasing the number
of repositions required to accurately mark the lesion.

The present invention relates to a needle assembly
25 for localization of lesions within the body, including a needle
cannula, said cannula having a cutting edge at a first end;
and a marking device positioned within said cannula and
including a shaft, said marking device being characterized
by a wire helically wound at one end of said shaft and
30 extending beyond said end a predetermined distance in a
helical coil, and having a sharpened tip, said marking device
being axially slidable and rotatable within said cannula.

The present invention further relates to a marking
device for use in combination with a needle assembly for
35 marking lesions within the body characterized
by a shaft; a first helically

- 1 coiled wire secured to and wound about a first end of
said shaft, said first wire extending concentrically
outwardly from said first end and away from said shaft
a predetermined length and terminating in a sharpened
5 tip; and a second helically coiled wire secured to and
wound about said shaft a distance from said first helically
coiled wire, said second wire having a length equal to
said predetermined length that said first wire extends
from said shaft; wherein said first and second helically
10 coiled wires are wound an equal number of turns of
between 6 and 15 turns per centimeter.

- The present invention also relates to a method
for marking non-palpable lesions within the body, charac-
15 terized by puncturing the skin to enter the body with a
marking needle assembly, said needle assembly including
a cannula having a lumen, a cutting edge at one end of said
cannula and a gripping means on said cannula, said needle
assembly further including a marking device positioned within
20 said lumen, said marking device having a helical wire
helically wound at one end a predetermined distance in a
helical coil, and having a sharpened tip; aid marking device
being axially slidable and rotatable within said cannula;
tracking said needle assembly inside said body; advancing
25 said needle assembly to a point within proximity to a lesion
within said body; rotating said marking device within said
cannula to advance said marking device; determining the
distance said marking device travels by the distance said
marking device is advanced into said cannula; ceasing rota-
30 tion of said marking device when said marking device is
positioned within a determined proximal distance of said
lesion; and removing said cannula from said body; wherein
said marking device remains in position with respect to said
lesion to mark said lesion for subsequent medical procedures.

1 The present invention will become more readily
apparent and may be understood by referring to the
following detailed description of the lesion localization
and marking device having a helically wound wire tip,
5 taken in conjunction with the accompanying drawings;
in which:

Figure 1 illustrates a side elevational view
of a marking device pursuant to the present invention;

Figure 2 illustrates a side elevational view
10 of a hypodermic needle or cannula pursuant to the
present invention;

Figure 3a illustrates an elevational end view of
the gripping knob of the hypodermic needle of Figure 2 along
15 lines 3a-3a;

Figure 3b illustrates an elevational end view of
the cannula of the hypodermic needle of Figure 2 along lines
3b-3b;

Figure 4 illustrates a perspective, partially
20 sectional view of the lesion localization needle assembly
pursuant to the present invention after insertion into the
body but prior to marking a lesion;

Figure 5 illustrates a perspective, partially
sectional view of the needle assembly of Figure 4 during
25 rotation of the marking device within the cannula and into a
lesion;

Figure 6 illustrates the needle assembly of Figure
4 after rotation of the marking device into the cannula with
the wire marker being fully embedded within a lesion;

Figure 7 illustrates a side elevational view of an
30 alternate embodiment of a marking device pursuant to the
present invention; and

Figure 8 illustrates a side elevational view of an
alternate embodiment of a needle or cannula pursuant to the
35 present invention.

1 Referring now in specific detail to the drawings,
in which identical reference numerals identify similar or
identical elements throughout the several views, Figure 1
shows marking device 10 according to the present invention.

5 Marking device 10 is constructed of a biocompatible material,
and is preferably constructed of stainless steel, although
many metal alloys such as aluminum alloy, titanium alloy,
ferrous alloy, and the like, as well as materials such as
plastic and ceramic, may be employed. Marking device 10

10 essentially consists of a shaft 12 which is preferably type
18-8 stainless steel having a thickness of between 0.011 and
0.20 inches diameter, and is preferably 0.016 inches
diameter. Marking device 10 is provided at one end with

15 helical marking wire 14 which is helically wound about the
end of shaft 12 and secured to the shaft as illustrated at
20. Preferably, helical marking wire 14 is constructed of
the same material as shaft 12, and is secured to the shaft by
soldering, preferably of a 98% tin and 2% silver solder.

20 Helical marking wire 14 is wound about shaft 12 and extends
outwardly away from the shaft to terminate in a sharpened tip
16. The diameter of the coil formed by helix 14 remains
constant along its length. Helix 14 extends from the end of
shaft 12 a distance of between 0.5 centimeters and 2

25 centimeters, and preferably extends 1 centimeter from the end
of shaft 12. The pitch of the coil is determined by the
number of turns per centimeter, which along with the length
of helix 14, is dependent upon the application for which the
marker is to be used. Different tissues within the body have

30 different degrees of strength and resiliency, some requiring
more force to anchor the marker 10 in place, and thus some
tissues require a device having more turns per centimeter
than other tissues. Accordingly, helix 14 generally is
provided with between 6 and 15 turns per centimeter, and

35 preferably it is provided with 8 turns per centimeter for
marking breast lesions.

1 Separated a distance "d" along shaft 12 from
helical marking wire 14 is helical guide wire 18 which is
also wound about shaft 12. Helix 18 is constructed of the
same material as helix 14 and shaft 12, and helical wires 14
5 and 18 are the same gauge wire, preferably having a diameter
of between 0.009 and 0.015 inches (0.02 and 0.04 cm). The
preferred diameter for helical wires 14 and 18 is 0.011

inches (0.027 cm) for marking breast lesions. Helix 18 is
10 secured to shaft 12 in a manner similar to helix 14. Helix
18 is of the same length as the length that helix 14 extends
from the end of shaft 12 to sharpened tip 16, and also has
the identical amount of turns per centimeter as helix 14, and
thus the same pitch to the coil formed by helix 18.

15 Distance "d" is dependent upon the length of the
hypodermic needle or cannula with which marking device 10 is
to be used. This will be described in greater detail below.

As can be seen in Figure 2, hypodermic needle 30
comprises a cannula 32 having a sharpened cutting tip 34 and
20 a gripping knob 36. Cannula 32, like marking device 10, is
constructed of biocompatible material, and is preferably
stainless steel. In a preferred embodiment, the cannula is
18-gauge thin wall stainless steel type 504, and has a length
from tip 34 to knob end 36 of between 3 and 15 centimeters,
25 depending upon the type and location of the lesion to be
marked. Knob 36 is preferably constructed of thermoplastic
material such as nylon and is secured to cannula 32 at end
38 by conventional means such as epoxy, adhesives, and the
like. Knob 36 may have a ridged gripping surface 44 which
30 aids the physician in handling the needle 30. Cannula 32 is
of course hollow and defines a lumen 33, as best seen in
Figure 3B.

1 Gripping knob 36 has a hole 46 bored through the
knob, which in the preferred embodiment aligns with lumen 33
of cannula 32 so that the cannula can extend through the hole
to face 37 of knob 36. In addition to hole 46, a second hole
5 47 is bored through knob 36, which is offset and parallel to
hole 46. A wire guide 40 passes through hole 47 and may be
secured within the hole by conventional means such as epoxy,
adhesives, and the like. Wire guide 40 passes through hole
47 and is bent at 41 along face 37 of knob 36 to form guide
10 bar 42. Wire guide 40 may also loosely and pivotably rest
within hole 47 so that guide bar 42 may be moved into and out
of engagement with shaft 12 of marker 10. As seen in Figure
3a, guide bar 42 partially covers hole 46 in knob 36 so as to
reduce the opening of hole 46. The reason for this will be
15 explained in greater detail below.

 Figures 4, 5 and 6 show needle and marker assembly
50 in various positions during use of assembly 50 in marking
a lesion within the body. Assembly 50 comprises marking
device 10 as shown in Figure 1 positioned within the lumen 33
20 of needle 30 as shown in Figure 2. The location of the
lesion within the body, such as non-palpable lesions found in
the breast or organs deep within the body, is determined
radiologically or ultrasonically in a non-invasive procedure.
In order to biopsy the lesion or remove it, the surgeon must
25 have an accurate location of the lesion prior to performing
the surgical procedure to minimize damage to tissue. The
accuracy of the location of the marker will obviate any need
for additional incisions, as well as avoid unnecessary tissue
removal, which benefits the patient both physically and
30 cosmetically. The use of a marking device such as in the
present invention is illustrated in Figures 4, 5 and 6.

1 As seen in Figure 4, the needle and marker assembly
50 is inserted into the body through the skin surface 52
until cutting tip 34 of cannula 32 is positioned proximate a
lesion or tumor 54. Marking device 10 is positioned within
5 needle 30 such that sharpened tip 16 of helical marking wire
14 is positioned adjacent to cutting tip 34 of needle 30.
The length of needle 30, as well as the length of shaft 12
and distance "d" between marking wire 14 and guide wire 18 is
determined by the depth or distance lesion 54 is from the
10 surface of the skin 52. Distance "d" is determined such that
when marking device 10 is within the lumen 33 of needle 30,
forward end 19 of helical guide wire 18 engages and rests
against guide bar 42, resulting in sharpened tip 16 being
adjacent to cutting tip 34.

15 Turning now to Figure 5, after cutting tip 34 is
positioned proximate to lesion 54, marking device 10 is
rotated about shaft 12 to advance helical marking wire 14
into lesion 54. Sharpened tip 16 enters lesion 54 and the
20 rotation about shaft 12 further advances marking wire 14 into
the lesion to firmly anchor it in place. The depth to which
helical marking wire 14 enters lesion 54 is determined by the
distance helical guide wire 18 travels through hole 46 into
cannula 32. As shaft 12 is rotated, guide bar 42 of wire
25 guide 40 engages the shaft and helix 18 at end 19 of helix 18
and guides shaft 12 while allowing helical guide wire 18 to
rotate into hole 46 in a screw-like fashion. Guide bar 42 is
positioned between the individual coils of helical guide wire
18 to prevent slipping or pulling on the shaft. Wire guide
30 40 may be secured in hole 47 or may be pivotably secured so
that guide bar 42 may rotated away from shaft 12 to disengage
guide bar 42 from helix 18.

1 When helical marking wire 14 is embedded and
anchored in lesion 54, that is when the end 23 of shaft 12 is
proximate to the lesion 54, the rotation is ceased. This is
best seen in Figure 6. The surgeon may determine when marking
5 wire 14 is in its desired position with respect to lesion 54
when guide wire 18 completely disappears into knob 36 past
guide bar 42. The trailing end 21 of guide wire 18 is the
same distance from the end 23 of shaft 20 as the distance
between forward end 19 of guide wire 18 and sharpened tip 16
10 of marking wire 14. When the surgeon determines that the
marking wire 14 is in proper position, such as when it is
completely embedded in the lesion, as evidenced by trailing
end 21 of helix 18 turning into knob 36, the surgeon may then
remove needle 30 from the body leaving marking device 10
15 firmly embedded in the lesion. Alternatively, when it is
determined that the helix 14 is in a desired position with
respect to lesion 54 without helix 18 being completely within
cannula 32, such as when a lesion is located proximate the
chest wall as determined by ultrasonic imaging, wire guide 40
20 may be pivoted to rotate guide bar 42 away from helix 18 to
allow for removal of needle 30 without disturbing the
position of helix 14. Marking device 10 remains firmly
anchored due to the concentric nature of the coils of marking
wire 14 and eliminates the possibility of inadvertent
25 dislodgement due to relaxation of the tissues of the breast
upon discontinuing the compression placed on the breast
during the procedure.

Figure 7 illustrates an alternate embodiment of the
present invention showing marking device 10a, in which helix
30 14a and helix 18a are integrally wound as part of shaft 12a.
Figure 7 is identical to Figure 1 in operation and function
except that additional helical wires are not needed, since

- 1 marking device 10a is of unitary construction in that shaft
12a and helixes 14a and 18a are constructed as a single unit.
In a further embodiment, helix 14 and helix 18 may be joined
so that the entire shaft 12 is in a helical coil.
- 5 In a further embodiment, cannula 32 may be provided
with a notched portion 60, and knob 36 may be eliminated, as
seen in Figure 8. In this case, notch 60 engages helix 18,
or alternately helix 14, dependent upon location of notch 60.
Notch 60 will then guide marking device 10 in the same manner
10 as wire guide 40 and guide bar 42.

While the invention has been particularly shown and
described with reference to the preferred embodiments, it
will be understood by those skilled in the art the various
changes in form and detail may be made therein without
15 departing from the spirit and scope of the invention.
Accordingly, modifications and/or changes such as removing
guide wire 18 or providing a longer or shorter marking wire,
as well as increasing or decreasing the pitch of the coils as
related to the number turns per centimeter, may be provided
20 as desired, and are considered to be within the scope of the
invention.

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-18-

1 WHAT IS CLAIMED IS:

1. A needle assembly for localization of lesions within the body, including a needle cannula, said cannula having a cutting edge at a first end; and a
5 marking device positioned within said cannula and including a shaft, said marking device being characterized by a wire (14; 14a) helically wound at one end (23; 23a) of said shaft (12; 12a) and extending beyond said end a predetermined distance in a helical coil, and having a
10 sharpened tip (16; 16a), said marking device (10) being axially slidable and rotatable within said cannula (32).

2. A needle assembly according to Claim 1, characterized in that said wire (14) is wound about and secured to said shaft (12).

15 3. A needle assembly according to Claim 1 or 2, characterized in that said cannula (32) and said marking device (10) are constructed of biocompatible material, such as stainless steel or a metal alloy.

4. A needle assembly according to any of Claims
20 1 to 3, characterized in that said helical coil of said wire (14; 14a) has a constant diameter along its length.

5. A needle assembly according to any of Claims 1 to 4, characterized in that said cannula (32) has a lumen (33); at least one notched portion (60) on said
25 cannula; said marking device (10) engaging said at least one notched portion, such that advancement of said marking

-19-

1 device is assisted by said helical wire (14; 14a) at one
end of said marking device rotatably contacting said at
least one notched portion.

6. A needle assembly according to any of Claims
5 1 to 5, characterized in that said cannula (32) has a
lumen (33), a cutting edge (34) at a first end of said
cannula, and a gripping knob (36) secured at a second end
of said cannula, said knob having a first hole (46) formed
therethrough in alignment with said lumen (33), and a
10 second hole (47) formed therethrough offset from said
first hole and having a wire guide (40) passing through
secured within said second hole in a direction parallel to
said cannula, said wire being bent at a right angle to
partially cover said first hole; said marking device (10)
15 further including a second helical wire (18) coiled about
said shaft (12) and secured thereto a distance from said
first helical wire (12) towards a second end of said
shaft; said second helical wire of said shaft engaging
said wire guide of said knob (36), such that the
20 advancement of said shaft is assisted by said second
helical wire (18) rotatably contacting said wire guide
(40).

7. A needle assembly according to Claim 6,
characterized in that said first and second helical wires
25 (14, 18) of said marking device (10) are secured to said
shaft (12) by soldering.

-20-

1 8. A needle assembly according to Claim 6 or 7,
characterized in that said first helical wire (14) extends
past said shaft end (23) a predetermined distance which is
equal to the length of said second helical wire (18).

5 9. A needle assembly according to any of Claims
6 to 8, characterized in that said second helical wire
(18) is positioned a predetermined distance from said
first helical wire (14), such that when an end of said
second helical wire closest to said first helical wire
10 engages said wire guide (40) of said knob (36), said
sharpened tip (16) of said first helical wire is
positioned coaxial and adjacent to said cutting edge of
said cannula.

15 10. A needle assembly according to Claim 8,
characterized in that an end of said second helical wire
(18) remote from said first helical wire (14) is
positioned at a distance such that when said second end is
rotated past said wire guide (40) into said cannula (32),
said first end of said shaft (12) is positioned coaxial
20 and adjacent to said cutting edge (34) of said cannula
(32).

25 11. A needle assembly according to any of Claims
6 to 10, characterized in that said first and second
helical wires (14, 18) have a constant diameter along
their entire lengths.

-21-

1 12. A needle assembly according to Claim 11,
characterized in that said first and second helical wires
(14, 18) have a diameter substantially equal to each other
and less than the diameter of said shaft (12) of said wire
5 marker (10).

13. A needle assembly according to Claim 12,
characterized in that said first and second helical wires
(14, 18) have a diameter of approximately 0.02 cm and said
shaft (12) has a diameter of approximately 0.04 cm inches.

10 14. A needle assembly according to any of Claims
8 to 13, characterized in that said predetermined distance
of said first helical wire (14) extends past said shaft
end and the length of said second helical wire (18) is
between 0.5 and 2.0 cm.

15 15. A needle assembly according to Claim 14,
characterized in that said predetermined distance is 1 cm.

16. A needle assembly according to any of Claims
6 to 15, characterized in that said first and second
helical wires (14, 18) are wound about said shaft (12) an
20 identical number of turns per centimeter.

17. A marking device for use in combination with
a needle assembly for marking lesions within the body,
according to any of the preceding claims, characterized by
a shaft (12); a first helically coiled wire (14) secured
25 to and wound about a first end of said shaft, said first
wire extending concentrically outwardly from said first

-22-

- 1 end and away from said shaft a predetermined length and
terminating in a sharpened tip (16); and a second
helically coiled wire (18) secured to and wound about said
shaft a distance from said first helically coiled wire,
5 said second wire having a length equal to said
predetermined length that said first wire extends from
said shaft; wherein said first and second helically coiled
wires are wound an equal number of turns of between 6 and
15 turns per centimeter.
- 10 18. A method for marking non-palpable lesions
within the body, characterized by puncturing the skin to
enter the body with a marking needle assembly, said needle
assembly including a cannula having a lumen, a cutting
edge at one end of said cannula and a gripping means on
15 said cannula, said needle assembly further including a
marking device positioned within said lumen, said marking
device having a helical wire helically wound at one end a
predetermined distance in a helical coil, and having a
sharpened tip; aid marking device being axially slidable
20 and rotatable within said cannula; tracking said needle
assembly inside said body; advancing said needle assembly
to a point within proximity to a lesion within said body;
rotating said marking device within said cannula to
advance said marking device; determining the distance said
25 marking device travels by the distance said marking device
is advanced into said cannula; ceasing rotation of said

-23-

1 marking device when said marking device is positioned
within a determined proximal distance of said lesion; and
removing said cannula from said body; wherein said marking
device remains in position with respect to said lesion to
5 mark said lesion for subsequent medical procedures.

19. A method according to Claim 18,
characterized in that said gripping means includes a
gripping knob having a first hole formed therethrough
aligned with said lumen and a second hole formed
10 therethrough offset and parallel to said first hole for
receiving a wire guide, said wire guide bent at an angle
perpendicular to said second hole and covering a part of
said first hole, said needle assembly further including a
marking device positioned within said lumen, said marking
15 device having a shaft and at least two helically wound
wires concentrically coiled about and secured to said
shaft and spaced from each other a predetermined distance,
a first helical wire secured at an end of said shaft and
concentrically extending outwardly a predetermined length
20 from said shaft and terminating in a sharpened end, and a
second helical wire coiled about said shaft having an
equal number of turns per centimeter as said first helical
wire, a first end of said second helical wire engaging
said wire guide while said sharpened end of said first
25 helical wire is adjacent to said cutting edge of said
cannula;

-24-

1 said rotating of said marking device within the
lumen of said cannula advancing said marking device such
that said wire guide draws said marking device through
said lumen by engaging said second helical wire;

5 determining the distance said first helical wire travels
by the distance said second helical wire has travelled
past said wire guide; ceasing rotation when said first
helical wire marks said lesion; and removing said cannula
from said body;

10 wherein said first helical wire remains in
position with respect to said lesion to mark said lesion
for subsequent medical procedures.

20. A method according to Claim 19,
characterized in that said rotation continues until said
15 first helical wire is embedded in said lesion and said
second helical wire passes fully into said knob beyond
said wire guide.

21. A marking device for implementing the method
according to any of Claims 19 or 20.

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1 / 3

FIG. 1

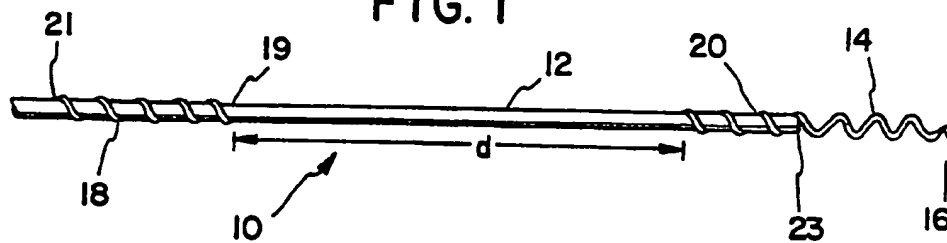


FIG. 2

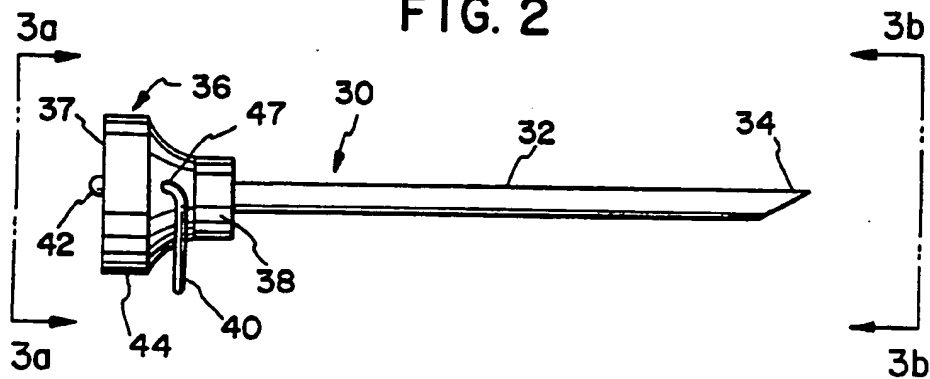


FIG. 3b

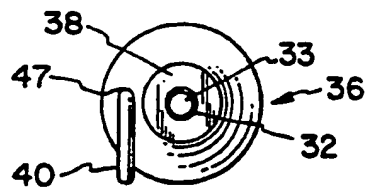
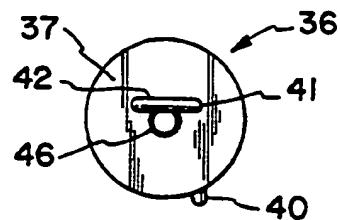


FIG. 3a



2 / 3

FIG. 4

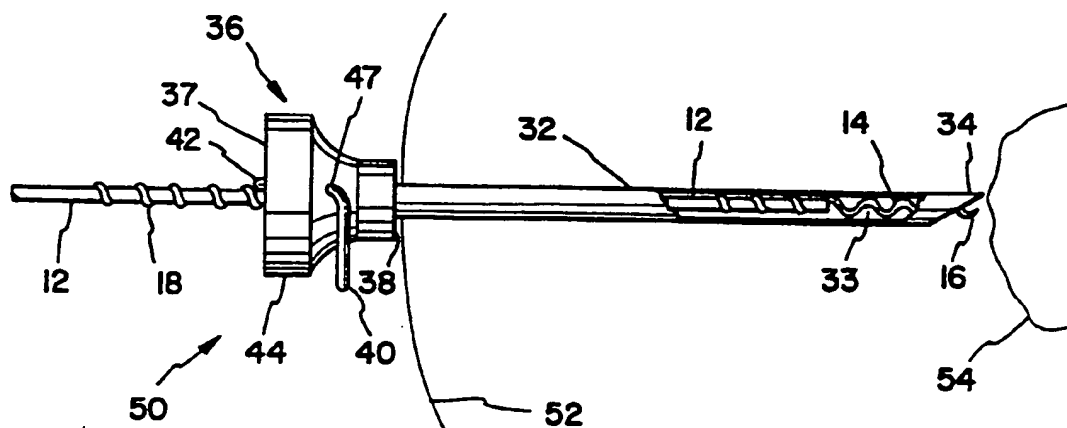
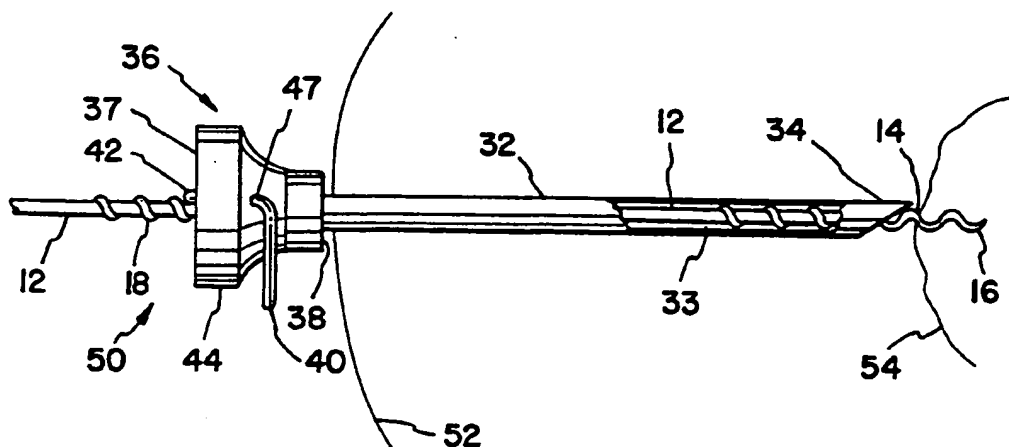


FIG. 5



SUBSTITUTE SHEET

3 / 3

FIG. 6

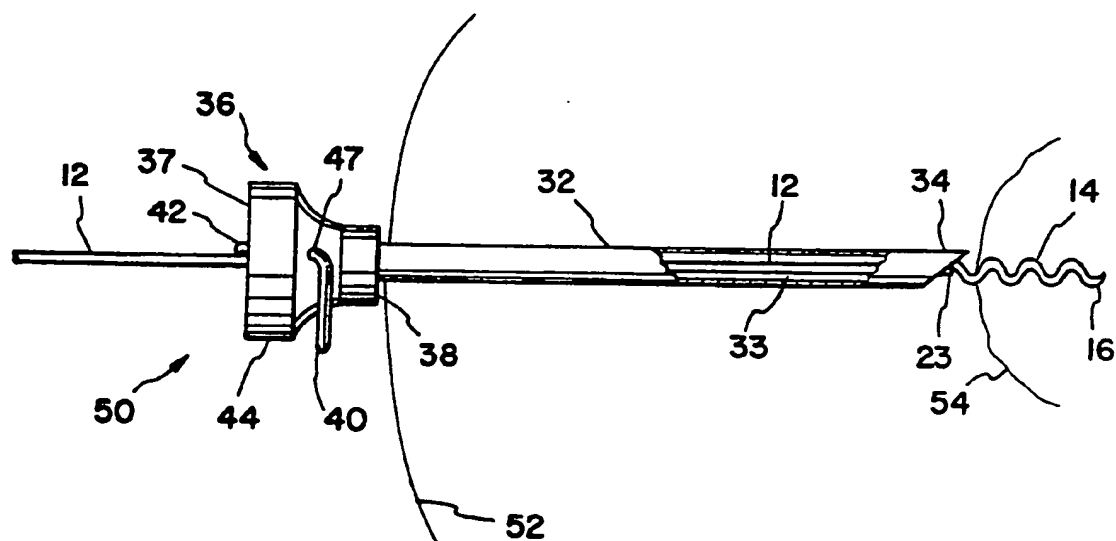


FIG. 7

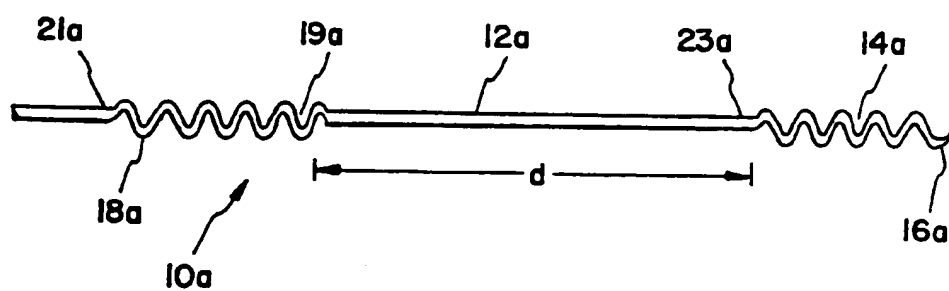
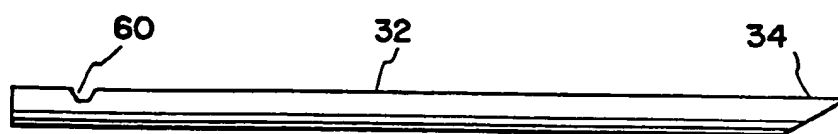


FIG. 8



SUBSTITUTE SHEET

INTERNATIONAL SEARCH REPORT

International Application No **PCT/US90/03244**

I. CLASSIFICATION OF SUBJECT MATTER (If several classification symbols apply, indicate all) *

According to International Patent Classification (IPC) or to both National Classification and IPC
IPC (5): A61B 10/00
U.S.Cl.: 128/749

II. FIELDS SEARCHED

Minimum Documentation Searched *

Classification System	Classification Symbols
U.S.Cl.	128/658,753,630,749,754 73/426-428 604/164 606/221-225,104,96,180 81/3.45

Documentation Searched other than Minimum Documentation
to the Extent that such Documents are Included in the Fields Searched *

III. DOCUMENTS CONSIDERED TO BE RELEVANT **

Category *	Citation of Document, ** with indication, where appropriate, of the relevant passages **	Relevant to Claim No. **
Y	US, A, 2,850,007 (LINGLEY) 02 September 1958 col. 2 lines 18-41	1, 3-6, 8-12, 14-16, 18
Y	US, A, 4,616,656 (NICHOLSON) 14 October 1986 col. 3 line 6	3
Y	Radiology 117, November, 1975 Nordenstrom page 474, line 5	3, 13
Y	US, A, 4,548,206 (OSBORNE) 22 October 1985 col. 3 lines 37-44	2, 7, 17, 21
Y	US, A, 4,658,678 (PRACHT) 21 April 1987 col. 3, lines 37-59	5
Y	US, A, 3,683,891 (ESKRIDGE et al.) 15 August 1972 col. 2, 3 lines 63 +	17, 21

* Special categories of cited documents: **

"A" document defining the general state of the art which is not
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which is cited to establish the publication date of another
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other means

"P" document published prior to the international filing date but
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"T" later document published after the international filing date
or priority date and not in conflict with the application but
cited to understand the principle or theory underlying the
invention

"X" document of particular relevance: the claimed invention
cannot be considered novel or cannot be considered to
involve an inventive step

"Y" document of particular relevance: the claimed invention
cannot be considered to involve an inventive step when the
document is combined with one or more other such docu-
ments, such combination being obvious to a person skilled
in the art.

"&" document member of the same patent family

IV. CERTIFICATION

Date of the Actual Completion of the International Search *

09 August 1990

Date of Mailing of this International Search Report *

02 OCT 1990

International Searching Authority *

ISA/US

Signature of Authorized Official NGOC-HO

For Robin R. Longo *Nguyen*
INTERNATIONAL DIVISION